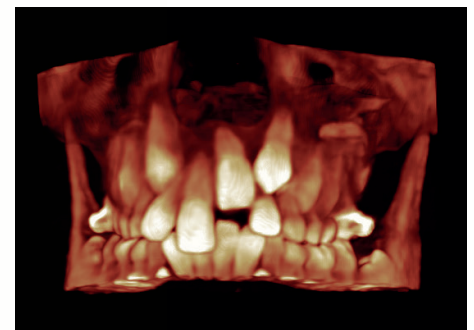


Planmeca Ultra Low Dose™

An average of **77% reduction in radiation dose** without statistical reduction in image quality.*

*"Dosimetry of Orthodontic Diagnostic FOVs Using Low Dose CBCT Protocol" by JB Ludlow and J Koivisto.



Effective dose: 4 μ Sv

PLANMECA

Pioneering low dose 3D imaging

Planmeca CBCT imaging units offer Planmeca Ultra Low Dose™ technology which reduces effective patient dose to levels comparable to, and often lower than traditional 2D imaging modalities.

More information, less radiation

Planmeca Ultra Low Dose™ can be selected on all volumes and resolution settings from Low Dose to Endodontic mode. Using the Planmeca Ultra Low Dose protocol reduces the effective patient dose by an average of 77% without a statistical reduction in image quality.*

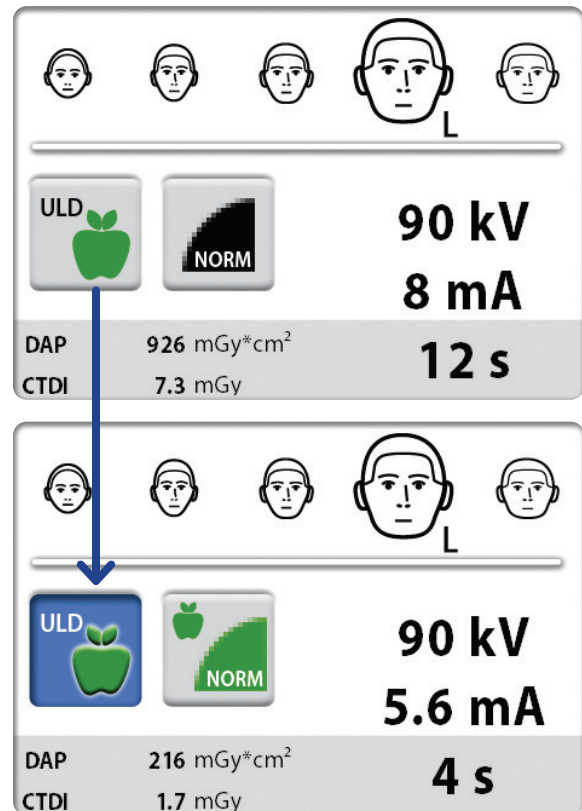
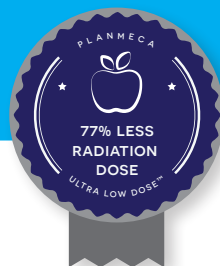
The unique and pioneering imaging protocol is based on intelligent 3D algorithms developed by Planmeca. Our 3D imaging system allows clinicians to always choose the optimal balance between image quality and dose, based on the ALADA principle.

Ideal for many clinical cases

The Planmeca Ultra Low Dose™ protocol has proven to be ideal for many clinical cases.

- Orthodontics:
 - Defining the amount of bone around the root
 - Localizing unerupted and impacted teeth before orthodontic treatment
 - Defining orthodontic landmarks for cephalometric analysis
- Post-operative and follow-up images in maxillofacial surgery
- Airway studies
- Sinus studies
- Implant planning

Learn more about Planmeca Ultra Low Dose™ by visiting www.planmeca.com/low-dose-3d-imaging










Background and Methodology

The dose measurements are performed using an anthropomorphic RANDO phantom and MOSFET dosimeters positioned into the phantom, according to the effective dose measurement protocol described by Ludlow et al. The effective dose calculation is based on using the revised guidelines given by the **International Commission on Radiological Protection (ICRP 103)**. At Planmeca, the Corporate Physicist Juha Koivisto is in charge of the effective dose measurements.

Planmeca 3D family

The optimal 3D unit for every imaging need.

		Normal mode		Low dose mode	
		Voxel size	 Effective patient dose with ULD	Voxel size	 Effective patient dose with ULD
	Planmeca ProMax® 3D s				
	Ø 5 x 5 cm – Tooth upper incisors	200 µm	17 µSv	400 µm	6 µSv
	Ø 5 x 8 cm – Tooth incisors	200 µm	22 µSv	400 µm	8 µSv
	Planmeca ProMax® 3D Classic and ProMax® 3D LE				
	Ø 8 x 8 cm – Teeth	200 µm	30 µSv	400 µm	9 µSv
	Planmeca ProMax® 3D Plus				
	Ø 9 x 9 cm – Teeth	200 µm	27 µSv	400 µm	7.9 µSv
	Ø 16 x 9 cm – Jaw	400 µm	24 µSv	600 µm	9.5 µSv
	Planmeca ProMax® 3D Mid				
	Ø 10 x 10 cm – Teeth	200 µm	40 µSv	400 µm	8 µSv
	Ø 20 x 10 cm – Jaw	400 µm	25 µSv	600 µm	10 µSv
	Ø 20 x 17 cm – Face	400 µm	39 µSv	600 µm	16 µSv
	Planmeca Viso™ G7 and Viso™ G5				
	Ø 10 x 10 cm – Teeth	450 µm	101 µSv	450 µm	20 µSv
	Ø 14 x 10 cm – Jaw	600 µm	61 µSv	600 µm	12 µSv
	Ø 16 x 16 cm – Face	600 µm	51 µSv	600 µm	10 µSv

Standard 2D panoramic effective patient dose is approximately 15 µSv.

Introduction

Use of ionizing radiation in diagnostic medical examinations has increased over the last 20 years to the point where the annual per capita dose to the US population from all sources has doubled. (1) The risk of this exposure is significant, and it has been estimated that from 1.5% to 2% of all US cancers may be attributed to computed tomography (CT) studies alone. (2) Use of CT scans in children delivering cumulative doses of about 50 mGy might almost triple the risk of leukaemia and doses of about 60 mGy might triple the risk of brain cancer. (3) The range of doses produced by dental CBCT units is large with some examinations approaching doses associated with medical CT imaging. (4) Dosimetry of CBCT examinations for pediatric patients has not been established for many units that are currently used in orthodontic imaging.

Objectives

The purpose of this study was to evaluate doses resulting from various combinations of field size and exposure parameters using child and adult phantoms on a Promax 3D Mid CBCT unit. A second aim was to acquire contrast/noise ratio (CNR) data and modulation transfer function (MTF) data to examine the relationship of these measures of image quality to examination dose.

Effective doses resulting from combinations of field size and exposure parameters that might be used for orthodontic diagnosis tasks were acquired using a Promax 3D Mid CBCT unit (Planmecca Oy, Finland). Specifically doses for a protocol involving reduced exposure and proprietary reconstruction called "ultra low dose" (ULD) was compared with standard exposures. Contrast to noise ratio (CNR) and modulation transfer function (MTF) were calculated as quantitative measures of image quality.

Methods

Doses resulting from various combinations of field size, exposure protocol, and child or adult anthropomorphic phantoms using the Promax 3D MID CBCT unit (Helsinki, Finland) were measured with Optical Stimulated Luminescent (OSL) dosimetry using previously validated protocols. (5-6)

Optical Stimulated Luminescence dosimeters (OSLDs) (NanoDot, Landauer, Glenwood, IL)

- Placed at 24 locations in 10-year-old child and adult phantoms (CIRS, Norfolk, VA) (figure 1).
- Multiple exposures made for each dosimeter run
- Dosimeters read 3 times with Microstar ii reader (Landauer, Glenwood, IL) – average dose used
- Dose values were adjusted for sensitivity of dosimeters to effective kV of x-ray source
- Doses divided by number of exposures to obtain dose per scan

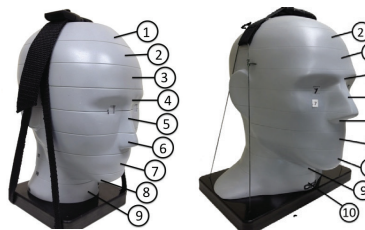


Figure 1. Child (left) and adult (right) dosimetry phantoms

Equivalent dose (H_T) determination

- Doses were determined in the organs and tissues listed in ICRP Report 103 (7)
- Average absorbed dose in each tissue or organ was used to calculate equivalent dose (H_T) $H_T = \sum W_R \times D_T$

Effective dose (E) determination

- Calculated in μSv as: $E = \sum w_T \times H_T$, where E is the product of the tissue weighting factor (w_T), which represents the relative contribution of that organ or tissue to the overall risk, and the equivalent dose (H_T).

Image Quality Assessment

- QUART DVT phantom and image reader (QUART GmbH, Munich, Germany) - used to measure CNR and MTF.

Analysis

- Standard and ULD image quality parameters were compared in a paired analysis.

Results

Table 1. Dose by phantom type, FOV, and protocol

Protocol	Phantom	volume (ø*h) in mm	Effective Dose in μSv
ULD Low Dose	Adult	100*100	12
ULD Normal			45
Low Dose			60
ULD Low Dose		200*170	189
ULD Normal			18
Low Dose			51
Normal	Child	85*85	72
ULD Low Dose			215
ULD Normal			10
Low Dose		200*170	36
Normal			48
ULD Low Dose			153
ULD Normal	200*170	15	
Low Dose		42	
Normal		74	
Normal			175



Figure 2. QUART phantom and analysis software display

Table 2. Image quality differences due to protocol and statistical p value of difference

	mean difference	prob > t
CNR	0.408	0.56
MTF 10%	0.038	0.56
MTF 50%	0.055	0.47

Conclusion

While the risk from dentomaxillofacial imaging is small for an individual, when multiplied by the large population of patients who are exposed to diagnostic imaging, radiation risk becomes a significant public health issue. Therefore, strategies to reduce patient dose, keeping doses "as low as reasonably acceptable" (ALARA) are desirable. An average reduction in dose of 77% was achieved using ULD protocols when compared with standard protocols. **While this dose reduction was significant, no statistical reduction in image quality between ULD and standard protocols was seen. This would suggest that patient doses can be reduced without loss of diagnostic quality.** Further investigation of the diagnostic efficacy of ULD scans in Orthodontic and Orthognathic surgical treatment planning is indicated.

References

- National Council on Radiation Protection and Measurements. Ionizing Radiation Exposure of the Population of the United States (Report No. 160), Bethesda, MD, 2009, The Council
- Brenner DJ, Hall EJ. Computed tomography-an increasing source of radiation exposure. N Engl J Med. 2007;357:2277-84
- Pearce MS, Salotti JA, Little MP, McHugh K, Lee C, Kim KP, Howe NL, Ronckers CM, Rajaraman P, W Craft AW, Parker L, Berrington de González A. Radiation exposure from CT scans in childhood and subsequent risk of leukaemia and brain tumours: a retrospective cohort study. Lancet 2012;380:499-505
- Ludlow JB, Timothy R, Walker C, Hunter R, Benavides E, Samuelson DB, Scheske MJ. Effective Dose of Dental Cone Beam CT - a meta analysis of published data and additional data for 9 CBCT units. Dentomaxillofac Radiol. 2014;44:20140197
- Ludlow JB, Ivanovic M. Comparative Dosimetry of Dental CBCT Devices and 64 row CT for Oral and Maxillofacial Radiology Oral Surg Oral Med Oral Pathol Oral Radiol Endodont 2008;106:930-938.
- Ludlow JB, Walker C. Assessment of phantom dosimetry and image quality of I-CAT FLX CBCT. American Journal of Orthodontics & Dentofacial Orthopedics 2013;144:802-17
- Valentin J. The 2007 Recommendations of the International Commission on Radiological Protection. Publication 103. Ann ICRP 2007; 37: 1-332

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